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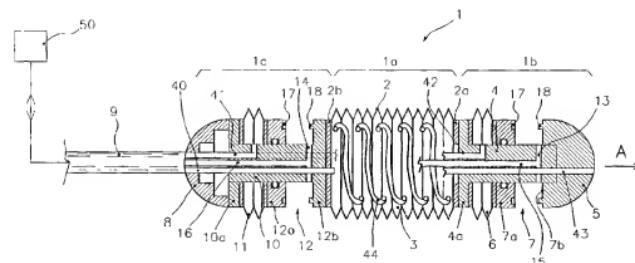
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(84) Title: ENDOSCOPIC DEVICE FOR LOCOMOTION THROUGH THE GASTRO-INTESTINAL TRACT



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(57) Abstract: An endoscopic device for locomotion in a body cavity according to a prefixed advancing direction (A) comprising at least a variable length intermediate section (1a, 21a) extending between a front end section (1b, 21b) and a rear end section (1c, 21c). First and second clamping means (7, 12, 27, 32) are integral to the front and rear section, for alternately grasping respective surrounding portions of wall (P) of the body cavity. Sucking means (13, 14, 37, 38) are associated to the first and second clamping means for creating a depression sufficient to cause the body cavity wall portions to collapse within the first and second clamping means while they are in an open condition. Means for actuating alternative extensions and retractions of the intermediate section and actuating means (6, 11, 26, 31) of the first and second clamping means are further provided for synchronous operation to generate a forward motion of the rear end section due to a retraction of the intermediate section, the wall portion (P) surrounding the first clamping means being firmly held therewith, and to generate a forward motion of the front end section due to an extension of the intermediate section, the wall portion (P) surrounding the second clamping means being firmly held therewith.

- 1 -

TITLE

ENDOSCOPIC DEVICE FOR LOCOMOTION THROUGH THE GASTRO-  
INTESTINAL TRACT

DESCRIPTION

5       Field of the invention

The present invention relates to an endoscopic device for locomotion through a tubular body cavity, in particular, but not exclusively, through the gastrointestinal tract, able to migrate in a prefixed direction  
10 with so-called inchworm motion.

Background of the invention

Endoscopic devices for surgical or diagnostic procedure are already known. These devices are operated by the surgeon who directly imparts to the device the forward  
15 motion through the patient's body. Surgical and/or diagnostic instruments which are necessary to carry out each specific procedure, such as microarms, microcameras, and/or laser emitters are generally associated to these devices.

20       In order to make easier the surgeon's task there have been proposed endoscopic devices of the above mentioned type capable of a semi-autonomous movement within the body cavity of a patient, adapting their shape, as far as possible, to the shape of the surrounding  
25 cavity. In this case, the walls of the body cavity act as a support for propelling the device forward. For example, in US-A-5398670 there is disclosed an endoscopic instrument substantially formed by a bellows-shaped tubular body, capable of extension and retraction, and by  
30 two end portions including respective inflatable balloon members, by means of which the front end portion and the rear end portion alternately engage by compression with

- 2 -

the walls of the body cavity through which the device must be pushed forward. There is provision for a control system which operates the inflation and deflation of the two balloon members and the extension and retraction of the 5 tubular body according to a sequence such as to produce the advancement of the device in the prefixed direction.

An endoscopic device of the same type is disclosed in US-A-5906591, in which, however, a vacuum pressure sufficient to produce, under the induced sucking 10 conditions, a substantial anchorage of the front and rear end portions to the cavity wall is created sequentially around these end portions.

When the endoscopic device of the type described in the above cited patents is destined to the locomotion 15 through the gastro-intestinal tract, its anchorage to the cavity walls is not satisfactory, because this type of cavity is soft, slippery and often wet. Using balloon-type endoscopic devices such that according to US-A-5298670, even if the intestinal wall is overextended, it is 20 impossible to produce sufficient traction forces due to extremely low friction coefficient of the gastro-intestinal tract. Furthermore, excessive overextension of the balloon will result in causing severe pain for the patient. A similar result is obtained by increasing the 25 suction in the case of the endoscopic device of US-A-5906591, with the drawback that, when the degree of vacuum is increased over a certain extent, undesirable lesions may appear.

In order to improve the anchorage of the endoscopic 30 devices of the above mentioned type it has proposed to equip them with auxiliary anchoring means of various shapes, which, however, increase the structural complexity

- 3 -

and the length of the device and increase the patient discomfort and the risk of damage of the involved tissues.

Summary of the invention

The object of the present invention is to provide an  
5 endoscopic device of the semi-autonomous locomotion type  
through a body cavity such as the gastro-intestinal tract,  
capable of assuring a suitable anchorage to the body  
cavity thereby allowing its advancement through it,  
without giving rise to any of the problems encountered  
10 with the similar known devices.

Another object of the present invention is to  
provide an endoscopic device of the above mentioned type  
for achieving a suitable anchorage to the cavity wall by  
means of structurally simple solutions allowing the size  
15 of the device to be kept small.

These object are reached with the endoscopic device  
for locomotion in a body cavity in a prefixed advancement  
direction according to the present invention, comprising  
at least a variable length intermediate section extending  
20 between a front end section and a rear end section with  
respect to said direction and first and second clamping  
means integral to the front end section and,  
respectively, the rear end section, for selectively  
grasping respective surrounding portions of the wall of  
25 the body cavity. Associated to the first and second  
clamping means suction means are provided for creating a  
vacuum sufficient to cause the surrounding portions of the  
body cavity walls to collapse within the first and the  
second clamping means, when they are in their open  
30 condition, to allow a firm grasping when said clamping  
means are closed. Means for operating alternate  
elongations and retractions of the intermediate section

- 4 -

and means for operating the first and second clamping means, synchronously operated to cause an advancement of the rear end section device in the prefixed direction following a retraction of the intermediate section when  
5 the respective portion of surrounding wall is firmly engaged with the first clamping means, and to cause an advancement of the front end section in the same direction following an elongation of the intermediate section when the respective surrounding wall portion is firmly engaged  
10 within the second clamping means.

Furthermore, the present invention provides a method for producing the locomotion through body cavities of an endoscopic device, by means of successive extensions and retractions of at least one variable length intermediate  
15 section thereof according a prefixed direction defining a front end section and a rear end section of the device, to which first and second clamping means are respectively associated selectively operable from the outside synchronously with the successive extensions and retractions of the intermediate section. The method is characterized by inducing selectively by suction a pneumatic depression in correspondence to one of the first or the second clamping means in their open condition, the depression being such that to cause the surrounding  
20 portion of body cavity wall to collapse within said clamping means, and closing said clamping means to grasp said surrounding wall portion and firmly anchoring to it the respective end section to allow the free movement of the other end section in the prefixed direction.  
25

30 The main advantage of the endoscopic device of the invention consists in that it can migrate through a tubular body cavity in every condition whatever the

- 5 -

available friction forces and the compliance of the body cavity are

Brief description of the drawings

Further characteristics and advantages of the 5 endoscopic device according to the invention will become more apparent from the following description of exemplifying, not limiting embodiments thereof, made with reference to the annexed drawings, in which:

- figure 1 is a longitudinal sectional view of a 10 first embodiment of the endoscopic device according to the present invention;
- figures 2a-2k show and advancement cycle of the device of figure 1;
- figure 3 is a longitudinal sectional view of a 15 second embodiment of the device according to the present invention;
- figure 4 is a cross sectional view of the endoscopic device of figure 3 taken along arrows IV-IV;
- figure 5 is a longitudinal sectional view of the 20 endoscopic device of figure 3 taken along arrows V-V of figure 4;
- figures 6a, 6b, 6c schematically show the operation of the clamping means integral to the rear end of the endoscopic device of figure 3;
- 25 - figures 7a, 7b schematically show the operation of the clamping means integral to the front end of the endoscopic device of figure 3;
- figures 8a-8g show and advancement cycle of the endoscopic device according to figure 3.

30 Description of the preferred embodiment

With reference to figure 1, it has been generally indicated at 1 an endoscopic device according to the

- 6 -

present invention. It comprises an intermediate section 1a of a tubular shape, extending between two end sections called front end section 1b and rear end section 1c, the terms "front" and "rear" being referred to a reference direction indicated at A. Clearly, the endoscopic device will be able to move in the body cavity in a forward and a backward direction. The tubular intermediate section 1a is formed by a wall 2 made of elastic and flexible material shaped like a bellows and delimiting a cavity 3 for containing a fluid, for example air. The intermediate section ends with a front flange 2a and a rear flange 2b through which it is connected to front end section 1b and rear end section 1c respectively.

Front end section 1b of the device is formed by a stem 4 fixed to front flange 2a at a flanged end 4a thereof and to a front head 5 of the device at the other end. Fixed to flanged end 4a of stem 4, at the opposite side of flange 2a, is a bellows member 6 which is integral to a jaw 7a of a first clamp 7 (also called front clamp) slidably mounted on stem 4 and fixed to the free end of bellows 6. The other jaw 7b of first clamp 7 is constituted by a face of front head 5 perpendicular to the axis of stem 4 and faced toward first jaw 7a.

Rear end section 1c is formed by a rear head 8, from which a tubular connector 9 extends, connected to a flanged end 10a of a stem 10. Fixed to flanged end 10a, at the opposite side of rear head 8, is a bellows member 11 integral to a jaw 12a of a second clamp 12 (also called rear clamp) coaxially and slidably mounted on stem 10, the other jaw 12b of second clamp 12 being formed by a plate fixed to the end of stem 10 at one side thereof and to rear flange 2b of intermediate section 1a at the other

- 7 -

side.

Tubular connector 9 puts into communication the device with an external control system, of the conventional type, for example as described and shown in 5 figure 3 of US-A-5906591, comprising a source (50) for selectively providing a positive or negative pressure to the various parts of the devices as will be explained below. More precisely, connector 9 houses pneumatic conduits extending in a substantially axial way within 10 device 1 (as schematically shown in figure 1), each of them being able to both feed compressed air to and suck air from chamber 3 of bellows-shaped intermediate section 1a (conduit 40), bellows member 6 and 11 controlling the operation of clamps 7 and 12 (conduits 41,42), as well as 15 to/from a surface portion of stems 4 and 10 comprised between jaws 7a, 7b and 12a, 12b, respectively, of clamps 7 and 12, through diametral ducts 13 and 14 extending from respective axial ducts 15 and 16 formed in stems 4 and 10, communicating with respective pneumatic conduits housed 20 within connector 9. A further pneumatic conduit 43 outflows from front head 5 to blow air jets useful to assisting forward motion of the device. In particular, pneumatic conduits passing through intermediate section 1a are helically arranged within chamber 3 as schematically 25 indicated at 44 in figure 1.

The operating cycle of the endoscopic device is now described with reference also to figures 2a-2k (the parts being in turn under pressure are shown as hatched). By creating suction conditions at rear clamp 12 a 30 substantially annular portion P of the surrounding wall of the body cavity is caused to collapse between jaws 12a, b which, by adduction of compressed air within bellows 11,

- 8 -

close against each other firmly grasping wall portion P (figure 2a). Through radial duct 13 of stem 4 air is blown against cavity wall P to cause its displacement from front end section 1b of the device (figure 2b). Then compressed air is fed to bellows 2 which elongates pushing front end section 1b of the device forward (figure 2c). At this point, a depression is created between jaws 7a, b of front clamp 7 which causes a substantially annular portion of the surrounding cavity wall P to collapse therebetween. By adducting compressed air bellows 6 is caused to elongate and clamp 7 closes firmly grasping cavity wall (figure 2e). Bellows 11 is then retracted by depression to open clamp 12 (figure 2f) releasing the grasped cavity wall which is displaced back from rear end section 1c of the device by means of air jets through radial duct 14 of stem 10 (figure 2g). Rear end section 1c is then pulled forward by bellows 2 which retracts due to depression induced therein (figure 2h). At this point, rear clamp 12 grasp a new annular portion of surrounding cavity wall P by creation of a depression between jaws 12a, 12b (figure 2i) and closure of rear clamp 12 (figure 2j), while front clamp 7 opens to release the grasped annular wall portion. Then the cycle is repeated with a new advancement step.

In order to improve the grip of jaws 7a, 7b and 12a, 25 12b of front clamp 7 and rear clamp 12 respectively, a circular groove 17 is formed on one of their opposed faces and a corresponding step 18 for engaging with groove 17 is formed on the other face. Advantageously all the edges of the grip surfaces are beveled to avoid any tissue damage.

30 A second embodiment of the endoscopic device according to the invention is shown in figures 3, 4, 5, 6a-c and 7a,b. In the figures, 21a indicates an

- 9 -

intermediate tubular section of the device formed by a bellows wall 22 made of elastic and flexible material delimiting a chamber 23, 21b indicates a front end section connected to intermediate section 21a through a front 5 flange 22a and 21c indicates a rear end section connected to intermediate section 21a through a rear flange 22b.

Front end section 21b comprises a head 25 connected to front flange 22a and integral to a stem 24 axially extending through intermediate section 21a and rear end 10 section 21c and connected to a tubular connector 29. A first clamp 27 is mounted at the end of stem 24 opposite to that where head 25 is fixed. Each clamp is formed by a jaw 27a axially slidable on stem 24 and by a jaw 27b fixedly connected thereto. Jaw 27a and 27b are each formed 15 by a pair of jaw portions diametrically arranged on stem 24. The two portions of jaw 27a are mutually connected by means of a bracket 28 passing through a slot 30 diametrically formed in stem 24. An actuating wire 26 crosses bracket 28 in two points and is fixed to the 20 bracket at one of them while being slidable at the other one. Wire 26 slidably extends through the overall length of stem 24 forming a loop along it and its free ends are conveyed externally through connector 29. Clearly, by pulling one of the two ends from the outside, the opening 25 and closure of clamp 27 can be controlled, as also shown in figures 7a and 7b.

As shown in figures 6a, b, c, rear end section 21c of the device comprises a first sleeve 33 coaxially mounted on stem 24 and slidable thereon. Sleeve 33 has a 30 flanged end one side of which is fixed to rear flange 22b of intermediate section 21a, the other one being fixed to a bellow 31 coaxial thereto. A pair of arm 33a, 33b extend

- 10 -

from sleeve 33 in a diametrically opposed and parallel relationship with respect to stem 24. Arms 33a, 33b are arranged on a plane rotated of an angle of 90° with respect to the two jaw portions of first clamp 27 and 5 support jaws 32a and 32b of second clamp 32. Likewise first clamp 27, second clamp 32 is formed by two diametrically opposed clamp portions and therefore clamps 27 and 32 are in a substantially crosswise arrangement with respect to the longitudinal axis of the device, as 10 shown in figure 4.

In particular, the pair of portions of jaw 32a are fixed to the free ends of arms 33a and 33b, while the pair of portions of mobile jaw 32b are formed at the end of two further arms 34a and 34b extending at the outside of arms 15 33a and 33b and parallel thereto from a second sleeve 34 integral to bellow 31 and axially slidable on sleeve 33. The sliding of arms 34a, b with respect to arms 33a, b is limited at one side by the abutment with fixed jaw 32a and at the other side by the mutual abutment between shoulders 20 35 and 36 formed on the respective sliding surfaces.

Tubular connector 29 houses a plurality of pneumatic tubes communicating to a series of conduits formed in stem 24. In particular, with reference to figure 3, conduits 37 and 38 are provided for creating a depression or feeding 25 compressed air between jaws 27a, b of first clamp 27 and jaws 32a, b of second clamp 32, to help engagement and, respectively, release of the surrounding wall portion P of the body cavity, and conduits 45 and 46 to suck or feed air from/to bellows 31 and 22, thereby causing them to 30 extend and respectively to retract. A conduit for feeding air to head 25 is also provided to blow air against the cavity wall during the forward motion. These conduits are

- 11 -

all shown in figure 3 for sake of simplicity. Conduits 38 and 45 are helically arranged inside chamber 23.

The operating cycle of the endoscopic device according to the second embodiment of the invention is shown in figures 8a-8g. First, vacuum is created in correspondance of the jaws of second clamp 32 to cause a surrounding wall portion P of the body cavity to collapse therebetween (figure 8a), then compressed air is entered in bellows 31 which in this way is elongated causing the closure of second clamp 32 and the grasping of wall portion P (figure 8b). Compressed air is entered in chamber 23 of bellows 22 which expands pushing front head 25 forward. In view of the connection through stem 24 front head 25 pull first clamp 27 forward (figure 8c). After having created a depression between the jaws of first clamp 27 to make the surrounding wall portion P to collapse therebetween, first clamp 27 is closed by traction of actuating wire 26 to grasp wall portion P (figure 8d). At this point second clamp 32 can be opened by sucking air from bellow 31, to release the wall portion P held thereby (figure 8e). Once second clamp 32 is opened, it is made to advance with respect to first clamp 27 by sucking air from bellow 22, which retracts (figure 8f). In these conditions, after second clamp 32 is held again to the body cavity wall, first clamp 27 is opened and the cycle repeated for a further advancement step.

Opposed grip surfaces of jaws of first and second clamp 27 and 32 are formed with an annular groove and a corresponding step for engaging therewith to improve the grip of the wall portion of the body cavity.

It will be appreciated that in the second embodiment of the invention clamps 27 and 32 alternately overtake

- 12 -

each other during each advancement step of the device and the clamp that in turn is in the distal position is the gripping one, while the other one is free and is pulled forward. This prevents the body cavity wall, due to its 5 easily yielding nature, from retracting into folds together with the device in the retraction step and extending in the next extension step without achieving any real forward motion of the device.

From the foregoing it is clear that the endoscopic 10 device according to the invention can migrate through a body cavity of tubular shape apart from the consistency of the walls and the friction that can be afforded by them, because it is able to grasp at the cavity wall before exerting its propulsive push. The increased patient's 15 comfort and the reduction of manual handling made possible with the device of the invention could promote the possibility of mass screening the population for gastro- 20 intestinal ailments, in particular to carry out colonoscopy and rectosigmoidoscopy, this being a particularly important inspection, in so far as about 70% of the colon cancers are localized in the first tract of the colon. In addition to inspection and diagnosis, future 25 integration of miniaturized endoscopic tools onboard the locomotive device would allow therapeutic procedures to be performed as well.

Several variations may be brought to the above described endoscopic device. Front and rear end sections can be removably connected to the intermediate section so as to be easily replaced in case of damage, for example 30 due to clogging by pollutants, or for maintenance. The wall of the intermediate section can be constituted by an elastically extensible smooth tube instead of a bellows.

- 13 -

The device could be made with disposable plastic materials, provided that they are suitable for insertion in a body cavity.

Even if in the present embodiments of the invention 5 pneumatically actuated bellows means have been provided for controlling the extension and the retraction of the intermediate section and the opening and closing of the clamping means, it is clear that, as an alternative, any equivalent linear actuating means such as elastic means or 10 minimotors, can be used. Likewise, compressed air distribution can be carried out in a different way from what has been illustrated, for example by using microvalves within the device, possibly controlled with shape memory alloy actuators.

15 Further variations and/or modifications can be brought to the endoscopic device according to the present invention, without departing from the scope of the invention as set forth in the attached claims.

- 14 -

CLAIMS

1. An endoscopic device for locomotion in a body cavity according to a prefixed advancing direction (A) comprising at least a variable length intermediate section (1a, 21a) extending between a front end section (1b, 21b) and a rear end section (1c, 21c) with respect to said direction and characterized in that it further comprises first and second clamping means (7, 12, 27, 32) integral to said front end section and, respectively, said rear section, for alternately grasping respective surrounding portions of wall (P) of said body cavity, and sucking means (13, 14, 37, 38) associated to said first and second clamping means for creating a depression sufficient to cause said body cavity wall portions to collapse within said first and second clamping means while they are in an open condition, means for actuating alternate extensions and retractions of said intermediate section and actuating means (6, 11, 26, 31) of said first and second clamping means being further provided for synchronous operation to generate a forward motion in said prefixed direction of said rear end section due to a retraction of said intermediate section, the wall portion (P) surrounding said first clamping means being firmly held therebetween, and to generate a forward motion of said front end section in the same direction due to an extension of said intermediate section, the wall portion (P) surrounding said second clamping means being firmly held therebetween.
2. The endoscopic device according to claim 1, wherein said first (7) and second (12) clamping means are arranged at opposite sides of said variable length intermediate section (1a)
3. The endoscopic device according to claim 1, wherein

- 15 -

said first (27) and second (32) clamping means are arranged at the same side of said variable length intermediate section (21).

4. The endoscopic device according to claim 3, wherein  
5 said first (27) and second (32) clamping means are arranged in correspondence of rear end section (21c) thereof.

5. The endoscopic device according to any one of claims 3  
and 4, wherein said first (27) and second (32) clamping  
10 means are arranged on two perpendicular planes and each comprises a pair of jaws being formed each by a pair of diametrical jaw portions.

6. The endoscopic device according to claims 1 or 2,  
wherein said front/rear end section (1b/1c) comprises a  
15 front/rear end head (5/8) and a respective stem (4,10)  
integral to it, to which a jaw (7b, 12b) of said  
first/second clamping means (7,12) is fixed, the other jaw  
(7a,12a) being slidably mounted on said respective stem  
(4,10).

20 7. The endoscopic device according to claim 6, wherein  
said actuating means of said first clamping means (7)  
comprise a pneumatically extendable and retractable  
bellows (6) integral to said slidable jaw (7a) and said  
intermediate section (1a).

25 8. The endoscopic device according to claim 6, wherein  
said actuating means of said second clamping means (12)  
comprise a pneumatically extendable and retractable  
bellows (11) integral to said slidable jaw (12a) and said  
rear head (8), said fixed jaw (12b) being integral to said  
30 intermediate section (1a).

9. The endoscopic device according to any one of claims  
1,3,4 or 5, wherein said front end section (21b) comprises

- 16 -

a front head (25) and a stem (24) integral to said head axially extending through said variable length intermediate section (21a) and said rear end section (21c), at the free end of said stem a jaw (27b) of said  
5 first clamping means (27) being fixed, the other jaw (27a) being slidably mounted on said stem (24).

10. The endoscopic device according to claim 9, wherein said actuating means of said first clamping means (27) comprise an actuating wire (26) operable from the outside  
10 fixed to said slidable jaw (27a).

11. The endoscopic device according to claim 10, wherein said actuating wire (26) is fixed to a bracket (28) axially slidable with respect to said stem (24) and integral to said slidable jaw (37a).

15 12. The endoscopic device according to any one of claims 1,3,4,5,9,10 or 11, wherein said rear end section (21c) comprises a first sleeve (33) integral to said variable length intermediate section (21c), a jaw (32a) of said second clamping means (32) being fixed to the free end  
20 thereof, the other jaw (32b) being formed at the end of a second sleeve (34) slidable on said first sleeve (33).

13. The endoscopic device according to claim 12, wherein said actuating means of said second clamping means (32) comprise a bellows (31) for connecting said first and  
25 second sleeve (33,34).

14. The endoscopic device according to any of the claims 12 or 13, wherein said first and second sleeve (33, 34) each comprises a tubular portion coaxial to said stem (24), respective pair of coplanar and diametrically opposed arms  
30 (33a,b; 34a,b) extending from said tubular portion for supporting said fixed jaw (32a) and, respectively, said slidable jaw (32b).

- 17 -

15. The endoscopic device according to any of the previous claims, wherein said sucking means comprise pneumatic conduits (13,14,37,38) formed within said stem (8,10,24) connected to a outside vacuum and compressed air source 5 (50) and outflowing between the jaws of said clamping means (7,12,27,32), said outside source being selectively operated to provide compressed air to be blown between said jaws when they open.
16. The endoscopic device according to any one of the 10 previous claims, wherein said intermediate section (1a, 21a) is formed by a flexible and elastic bellows body (2,22) defining a chamber (3,23) and said means for actuating alternate extensions and retractions of said intermediate section (1a, 21a) comprise a pneumatic 15 conduit (40,46) formed in said stem (10,24) and communicating with said chamber (3,23) and said outside vacuum and compressed air source (50) respectively.
17. The endoscopic device according to any one of the claims 7,8 or 13, wherein said bellows (6,11,31) 20 communicate through respective pneumatic conduits (41,42,38) with said outside vacuum and compressed air source (50) for selectively feeding compressed air or creating a depression therein to cause their extension or retraction.
25. 18. The endoscopic device according to any one of the previous claims, wherein said front end section (1b, 21b) is provided with means, for blowing compressed air in said body cavity to cause the surrounding wall thereof to spread apart during the forward motion, connected through 30 a pneumatic conduit (43,47) to said outside source (50).
19. Method for the locomotion of an endoscopic device through a body cavity, by means of a succession of

- 18 -

extensions and retractions of at least one variable length intermediate section (1a, 21a) in a prefixed direction (A) defining a front end section (1b, 21b) and a rear end section (1c, 21c) of said device, first and second clamping means (7,12,27,32) being associated to said front and, respectively, rear end section, said first and second clamping means being selectively operable from the outside synchronously to said extensions and retractions of said intermediate section, said method being characterized in  
5 that a pneumatic depression is selectively induced by suction in correspondance to one of said first (7,27) or second (12,32) clamping means in their open conditions, said depression being such that the surrounding wall portion (P) of said body cavity is caused to collapse  
10 within said clamping means, said clamping means being then closed to grasp said surrounding wall portion (P) and firmly hold one respective end section (1b,1c,21b,21c) thereto, thereby allowing the free movement of the other end section in the prefixed direction due to extensions  
15 and retractions of the intermediate section.  
20. The method according to claim 19, comprising a series of advancing cycles, each having the following steps:

- inducing said pneumatic depression by suction in correspondance to said second clamping means (12,32) in  
25 their open condition, thereby causing the surrounding wall portion (P) to collapse therewith;
- closing said second clamping means (12,32) to grasp said surrounding wall portion;
- extending said variable length intermediate section  
30 (1a, 21a) from a retracted condition to an extended condition;
- inducing said pneumatic depression by suction in

- 19 -

correspondance to said first clamping means (7,27) in their open conditions to cause the surrounding wall portion (P) to collapse therewith;

5 - closing said first clamping means (7,27) to grasp said surrounding wall portion therewith;

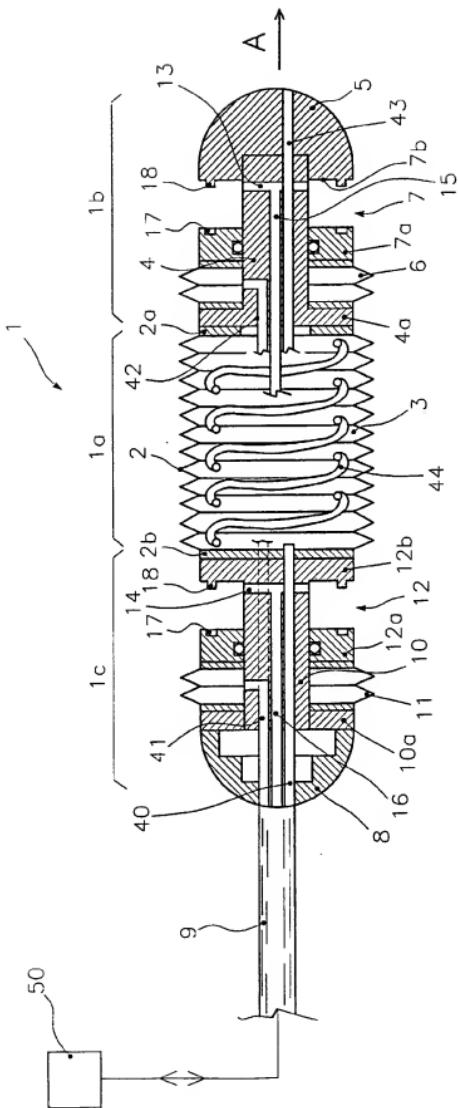
- opening said second clamping means (12,32) to release said surrounding wall portion therefrom;

10 - retracting said variable length intermediate section (1a,21a) from said extended condition to said retracted condition.

21. Method according to claims 19 or 20, wherein, after each opening step of said clamping means to release said surrounding wall portion, air is radially blown against it to enlarge said body cavity.

15 22. The method according to claims 19, 20 or 21, wherein the extension or retraction of said variable length intermediate section are performed by adduction or, respectively, suction of a fluid to/from a chamber (3,23) defined in said intermediate section, which is made of a  
20 substantially deformable material.

23. The method according to claim 22, wherein said fluid is air.

Fig.1

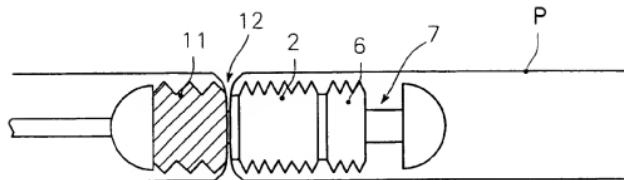


Fig. 2a

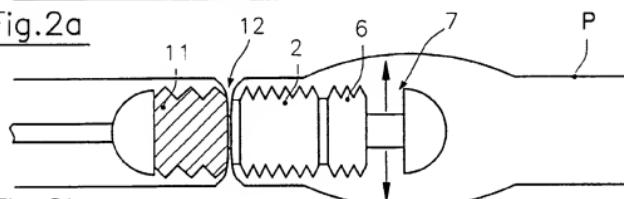


Fig. 2b

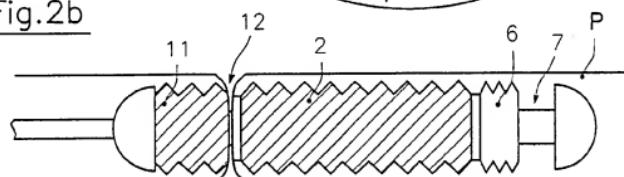


Fig. 2c

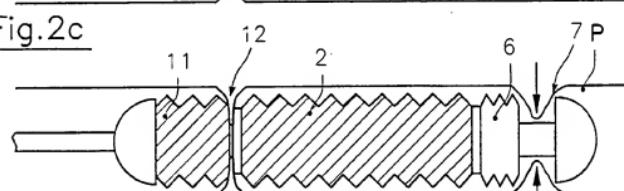


Fig. 2d

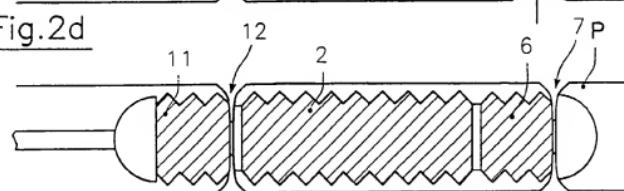


Fig. 2e

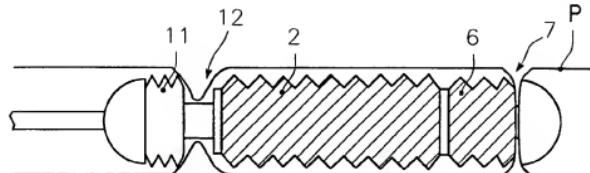


Fig.2f

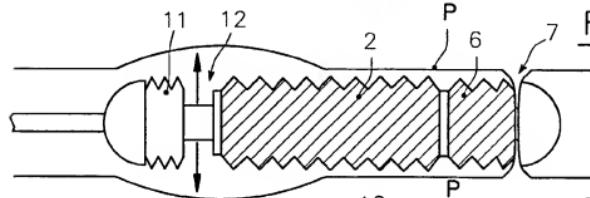


Fig.2g

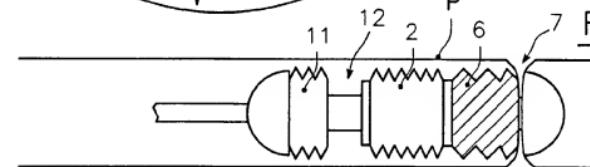


Fig.2h

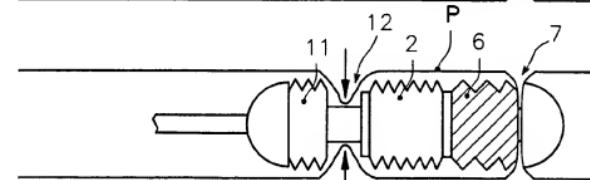


Fig.2i

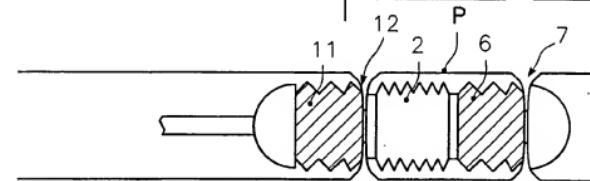


Fig.2j

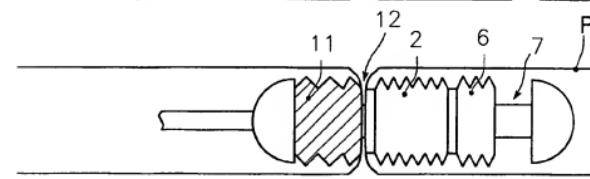


Fig.2k

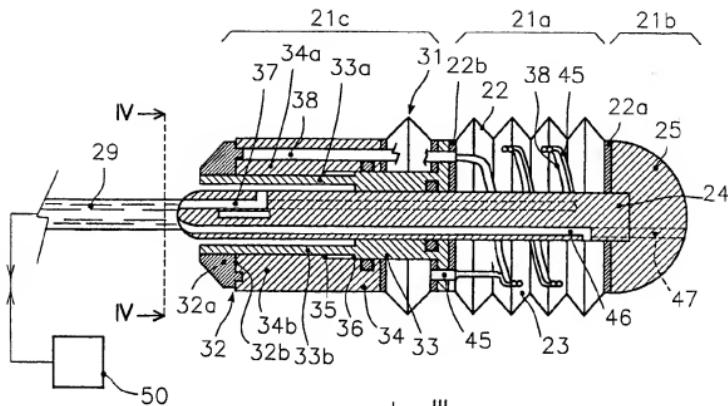


Fig.4

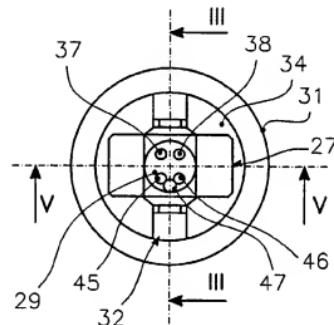
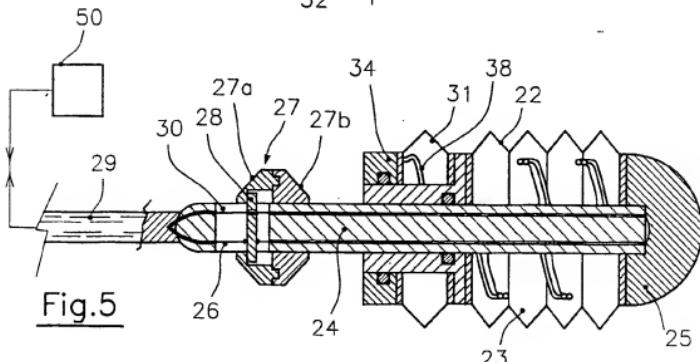
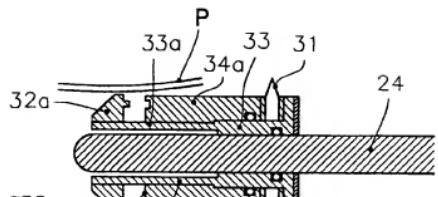
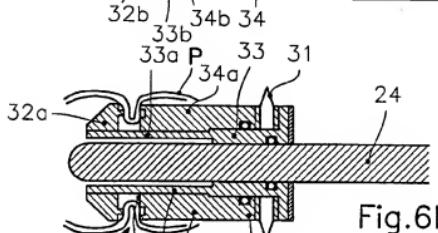
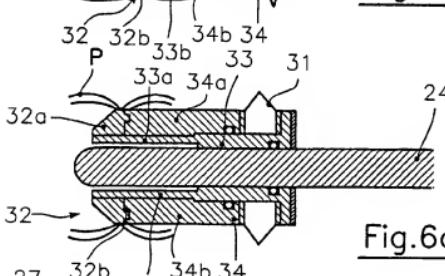
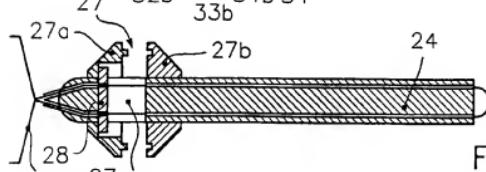
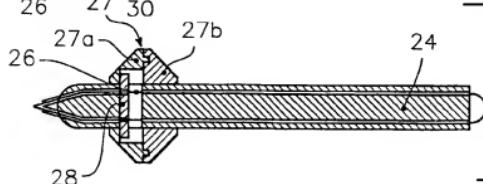


Fig.5



Fig.6aFig.6bFig.6cFig.7aFig.7b

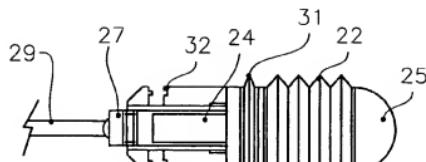


Fig. 8a

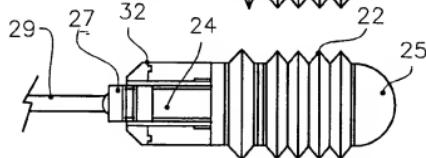


Fig. 8b

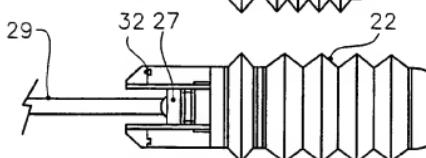


Fig. 8c

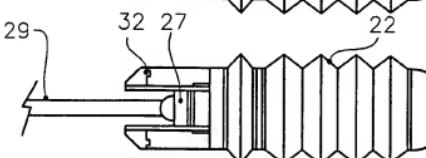


Fig. 8d

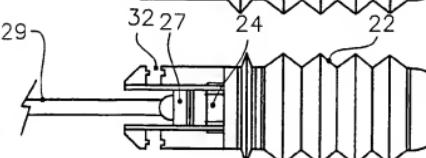


Fig. 8e

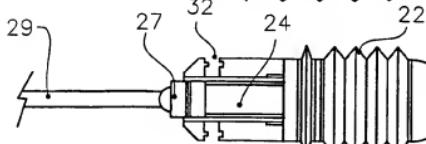


Fig. 8f

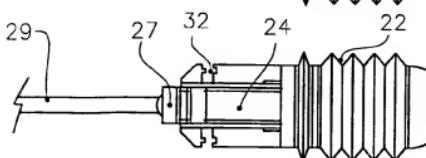


Fig. 8g

## INTERNATIONAL SEARCH REPORT

International application No.  
PCT/KR 01/00304

CLASSIFICATION OF SUBJECT MATTER		
IPC <sup>7</sup> : A61M 25/01, 25/08; A61B 1/00		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols)		
IPC <sup>7</sup> : A61B 1/00; A61M 25/01, 25/08, 25/082, 25/085		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)		
WPI, EPODOC, PAJ		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5398670 A (Ortiz M. et al.) 21 March 1995 (21.03.95) <i>the whole document; especially abstract; figures 3, 7A-7E (cited in the application).</i>	1
A	US 5906591 A (Dario P. et al.) 25 March 1999 (25.03.99) <i>the whole document; especially abstract; figures 1, 2A-2H (cited in the application).</i>	1
A	US 4389208 A (LeVeen R. et al.) 21 June 1983 (21.06.83) <i>the whole document; especially abstract; figures 2,5-8.</i>	1
A	US 4176662 A (Frazer R.) 4 December 1979 (04.12.79) <i>the whole document; especially abstract; figures 1,3.</i>	1
A	US 5364353 A (Corfitsen M. et al.) 15 November 1994 (15.11.94) <i>the whole document; especially abstract; figures 2-6.</i>	1
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<input type="checkbox"/>	Further documents are listed in the continuation of Box C.	<input checked="" type="checkbox"/> See patent family annex.
<input type="checkbox"/> Special categories of cited documents: „A“ document defining the general state of the art which is not considered to be of particular relevance „E“ earlier application or patent but published on or after the international filing date „L“ document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) „O“ document referring to an oral disclosure, use, exhibition or other means „P“ document published prior to the international filing date but later than the priority date claimed		„T“ later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention „X“ document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone „Y“ document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art „E“ document member of the same patent family
Date of the actual completion of the international search <b>24 January 2002 (24.01.2002)</b>		Date of mailing of the international search report <b>28 February 2002 (28.02.2002)</b>
Name and mailing address of the ISA/AT Austrian Patent Office Kohlmarkt 8-10; A-1014 Vienna Facsimile No. 1/53424/535		Authorized officer <b>LUDWIG</b> Telephone No. 1/53424/340

**INTERNATIONAL SEARCH REPORT**International application No.  
PCT/KR 01/00304**Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)**

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1.  Claims Nos.: 19 - 23  
because they relate to subject matter not required to be searched by this Authority, namely:  
**to a method for treatment of the human body by surgery regarding PCT-Rule 39 (iv)**
  
2.  Claims Nos.:  
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:
  
3.  Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

**Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)**

This International Searching Authority found multiple inventions in this international application, as follows:

1.  As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2.  As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3.  As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:
  
4.  No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

**Remark on Protest**

- The additional search fees were accompanied by the applicant's protest.  
 No protest accompanied the payment of additional search fees.

## INTERNATIONAL SEARCH REPORT

International application No.  
PCT/KR 01/00304

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US A 4176662	04-12-1979	none	
US A 4389208	21-06-1983	none	
US A 5364353	15-11-1994	DE C0 69219891 DE T2 69219891 DK A0 320/91 EP A1 591220 EP B1 591220 JP T2 6505176 JP B2 3131444 WO A1 9214507	26-36-1997 02-31-1998 25-32-1991 13-04-1994 21-05-1997 16-36-1994 31-01-2001 03-09-1992
US A 5398670	21-03-1995	none	
US A 5906591	25-05-1999	EP R2 838200 EP A3 838200 IT A1 962188 IT B1 1285533 JP A2 10216076	29-04-1990 20-10-1999 22-04-1998 08-06-1998 18-08-1998